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SWITCHABLE LENS

Abstract:

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A lens assembly (1) comprises a lens (2; 10, 11; 20) the focal length of which may be changed by application of an electric or magnetic field. A switching means (4, 15) provides a drive impulse to change the focal length of the lens (2; 10, 11; 20). An integral power source (4, 15) provides power for the switching means. A lens which can be switched between near and distance vision by the user is thereby provided.

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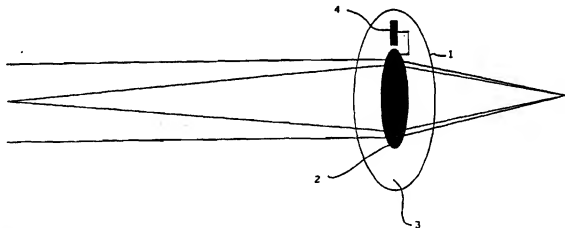
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(54) Title: SWITCHABLE LENS



(57) Abstract

A lens assembly (1) comprises a lens (2; 10, 11; 20) the focal length of which may be changed by application of an electric or magnetic field. A switching means (4, 15) provides a drive impulse to change the focal length of the lens (2; 10, 11; 20). An integral power source (4, 15) provides power for the switching means. A lens which can be switched between near and distance vision by the user is thereby provided.

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SWITCHABLE LENS

The present invention relates to a lens whose properties are variable.

5       The present invention has particular applicability in the area of bifocal lenses, and especially those used in ophthalmic applications, particularly contact lenses or intra-ocular lenses. Traditionally, contact and intra-ocular lenses have used a number of different techniques to  
10       allow users to see both near and distant objects. These techniques can be summarised as:

(i) Monovision - the user has lenses providing different focal lengths in each eye, one for near and one for distance vision.

15       (ii) Simultaneous vision - the eye of the user has both near and distant images focused on the retina simultaneously and the brain learns to distinguish the images and ignore the unwanted one; this may be achieved by the use of area division of the lens, polarisation  
20       division, chromatic division, or bifocal diffractive lenses.

(iii) Translating bifocals - a prism ballast is incorporated to orientate the lens correctly in the eye. The lens moves up and down across the cornea depending on  
25       whether the eye looks up or down. When looking down, the user sees through a different optical power.

All of these techniques have particular disadvantages. The first two share the common disadvantage that the user is continuously confronted with two images. In many  
30       situations, this compromises the quality of vision. A particular example is that of driving at night, when the user sees both focused and blurred oncoming headlamps simultaneously which leads to an inability to see the road ahead clearly. Translating bifocals are based on the  
35       assumption that, when looking straight ahead, the user needs only distance vision and that, when looking down, the

user needs only near vision. This is not always the case and is disadvantageous in many circumstances.

This invention aims to overcome these problems by providing a lens which can be switched between near and distance vision by the user. In the case of contact or intra-ocular lenses, the lens can be switched by the wearer; the user is therefore given the flexibility of a bifocal lens with the visual acuity of a monofocal lens.

The invention also has application in broader areas of optics. For example, it can provide a lens of variable focal length for use in compact disc players or optical memory disc drives.

According to the present invention, there is provided a lens assembly comprising:

a lens having a property which may be switched by application of an electric or magnetic field, said property being at least one of the focal length, absorption, colour, and effective aperture;

switching means to provide a drive impulse to switch the property of the lens; and,

an integral power source to provide power for the switching means.

The power source may be a conventional miniature battery or a photocell, for example. In this latter case, the unit has no power source other than the light incident upon it. In its primary intended application as an ophthalmic lens, the power source may be a battery operable using the tear fluid for its activation.

In one preferred embodiment where the lens is used as an ophthalmic lens, the user can control the lens assembly by a deliberate (voluntary) eye action that is distinct from usual normal eye actions. An example of this is an extended blink. A normal involuntary blink lasts around 1/10 sec. A deliberate, longer blink (conveniently not so long as to look unnatural) could provide a trigger for the lens to change focal length. For implementations employing

a photocell as power source, in very dark conditions, when the device is powered only to a very low level by the incident illumination, it can for example conveniently revert to a focal length which will provide distance vision.

It should be noted that the word "switch" is used in the following text primarily to refer to a change from one of two binary imaging states to the other. However, it should be read also to include an analogue change intermediate between those binary states. Such analogue switching could be useful in some applications (e.g. technical optics) where variable focal length, colour or aperture are desirable. For example, a variable focal length lens would have application in focus servo systems used in compact disc players.

The present invention is described in detail below only with reference to ophthalmic applications, although other applications should be understood.

Examples of the present invention will now be described with reference to the accompanying drawings, in which:

Fig. 1 is a schematic elevation of a lens assembly showing the general principles of the present invention;

Fig. 2 is an elevation of a first example of a lens assembly according to the present invention; and,

Fig. 3 is an elevation of a second example of a lens assembly according to the present invention;

Fig. 4 is an exploded elevation of the second example of a lens assembly shown in Figure 3;

Fig. 5 is a circuit diagram of a switching circuit; and,

Fig. 6 is a diagram showing a battery.

In Figure 1, there is shown a lens assembly 1 comprising an inner switchable lens 2 surrounded by a protective outer coating or lens 3 which encapsulates the switchable lens 2. A power source 4 is connected via circuitry 5 to the switchable lens 2 and allows the focal

length, absorption, colour or effective aperture of the switchable lens 2 to be switched.

A particular example of the present invention is illustrated in Figure 2, this first example being particularly suited to intra-ocular lenses where the lens has a relatively large centre thickness. A birefringent lens 10 made from a fixed birefringent material (which may be of conventional refractive, Fresnel or diffractive form) is placed optically in series with a liquid crystal cell 11, consisting of a liquid crystal layer 12 and a polariser layer 13. The birefringent lens 10 and the liquid crystal cell 11 are encased in a protective outer layer 14. A photocell and electronics circuitry 15 are provided within the protective outer layer 14 and are electrically connected to the liquid crystal layer 12.

The birefringent lens 10 produces a different focal length for each polarisation of light incident upon it, as is well understood. The liquid crystal cell 11 may have the property that it may select one of the polarisation states of light incident on it according to the electric field applied to the liquid crystal cell 11 by the photocell and circuitry 15. Consequently, the liquid crystal cell 11 may be used effectively to select either of the focal lengths of the birefringent lens 10. In the example shown in Figure 2, the unwanted polarisation state is absorbed by the polariser layer 13. The polariser layer 13 may be a layer separate from the liquid crystal layer 12.

Alternatively, the liquid crystal layer 12 may, by addition of a dichroic dye, in one state itself preferentially absorb one polarisation, obviating the requirement for the distinct polariser layer 13. In this case, when the liquid crystal in the liquid crystal layer 12 is undriven, one polarisation of light is absorbed and the assembly 1 behaves as a monofocal lens (with focus selectable, as described in more detail below, to be one of the foci produced by the birefringent lens); when the

liquid crystal in the liquid crystal layer 12 is driven, neither polarisation of light is absorbed and the assembly 1 has two foci, so it behaves as a simultaneous vision device in that state.

5 In another alternative implementation, the liquid crystal layer 12 may be a cholesteric liquid crystal doped with a dichroic dye, such that in the undriven state the cell is dark or coloured (depending upon the absorption characteristics of the dye) and, in the driven state, the  
10 cell may be transparent. In this way, a lens of variable absorption or colour may be constructed. If the cell is further divided into locally driven regions, the lens may be made with an effectively variable aperture. An example of this geometry is to provide switchable absorption in an  
15 outer annulus of the lens. This can provide a lens whose focal length is fixed but whose optical resolution and depth of focus can be controlled.

In order to test the viability of the first example described with reference to Figure 2, an assembly (not  
20 shown) has been constructed consisting of a liquid crystal lens as the birefringent lens 10, a switchable liquid crystal layer 12, a polariser layer 13, photodiodes and an external switch. The liquid crystal lens 10 was constructed as a cell with one flat side and one  
25 spherically curved side, with a maximum height of 80 microns and a diameter of 8mm. The lens cell walls were made of the ophthalmic plastics CR39, and filled with the high birefringence nematic liquid crystal Merck E44. The lens demonstrated two foci with optical powers of  
30 approximately 0 and +3 Dioptres. An unpatterned commercial twisted nematic liquid crystal cell with 25mm by 25mm active area and one polariser in place was then placed optically in series with the lens. This cell demonstrated a switching voltage of 5V. Twelve photodiodes were placed  
35 electrically in series to provide a DC supply to the cell via a manual switch. The finished device, powered by ambient light, has been demonstrated and a switchable



adjustment between optical powers of approximately 0 and +3D have been measured, even in dim room lighting.

A second form of device according to the present invention, which is of particular interest for applications requiring a thinner structure such as contact lenses, is to construct the lens itself as a switchable device. Figures 3 and 4 illustrate an example of this. The lens assembly 20 in this example includes a diffractive lens 21 formed of an isotropic material, perhaps by moulding, having annular steps 22 which provide the diffraction structure. A second isotropic component 23 forms a surface which matches the first except in the region of the diffractive structure formed by the annular steps 22. These two components 21, 23 together form a thin cell which contains a liquid crystal 24 in the spaces between the annular steps 22 and the second component 23. A photocell and electronics circuit 25 are provided in a further space between the isotropic components 21, 23 towards the periphery of the lens assembly 20.

In one example of the second form, the liquid crystal 24 is a nematic liquid crystal and is disposed so that, in its electrically unswitched state, either the ordinary or extraordinary refractive index of the liquid crystal is matched to that of the isotropic material of the components 21, 23. For one polarisation, therefore, illumination passes through the structure without angular deviation by the diffractive lens structure and therefore passes to a focus defined solely by the refractive lens form. The angular deviation produced by the diffractive lens structure for the other, deviated, polarisation varies across the aperture of the lens to produce a second distinct focus for this polarisation. When the liquid crystal layer 24 is electrically switched by use of the photocell and electronics circuit 25, the refractive index of the liquid crystal becomes polarisation-insensitive and the lens produces only a single focus.

A polariser (not shown) may be provided in addition to the diffractive lens, so that the device can be arranged to switch from one monofocal state (for example 0D) to another monofocal state (say +3D), producing a true monovision switchable lens with two selectable foci. Where the liquid crystal cell does not contain a separate polariser, in one state both foci are simultaneously produced and in that state the device behaves like a simultaneous vision lens, whilst in the other state (conveniently the distance-vision state), only one focus is produced.

According to a distinct, preferred embodiment of the invention, the lens assembly is an ophthalmic lens, preferably a contact lens, that is switchable between two states having different fixed focal lengths, independent of polarisation, by the application of an electric field. For this embodiment, the contact lens transmits at least 90% of incident light, and preferably nearly 100% of incident light, at each of the two focal lengths. The two focal lengths will normally correspond to desired near and distance vision corrections for the user.

The lens assembly of Figures 3 and 4 may contain a cholesteric liquid crystal instead of a conventional nematic. Cholesterics are nematics which are doped with a compound which forces the nematic molecular axes to form a helical structure. Such a structure does not significantly discriminate between polarisation states if the product of the twist pitch and the birefringence is small, typically less than one wavelength of light. When the cholesteric material is driven with an applied field, it switches to a second non-birefringent state of different refractive index in a similar way to conventional twisted nematic liquid crystals. Accordingly, a diffractive lens constructed in this way is a true monovision switchable lens (since a single, switchable focus is always provided), but is also independent of polarisation. Since it requires no additional polarisers (that absorb typically half of the incident illumination), it always transmits practically

100% of incident light, thus providing greater visibility for the wearer in low lighting conditions.

The lens assembly of Figures 3 and 4 may contain a liquid crystal material which is at a temperature above the clearing point of the material. At the clearing point, the material becomes isotropic, so that its refractive index is effectively the average of the ordinary and extraordinary indices. When the material is switched, the material aligns with the applied field and light passing normally through the material sees only the ordinary refractive index. Accordingly, a diffractive lens constructed in this way behaves as a true monovision switchable lens, and its properties are independent of the polarisation state of the light passing through it.

The diffractive lens of Figures 3 and 4 is preferably designed such that there is a full wavelength phase mismatch at the boundary of the zones of the diffractive lens, such that the light is deviated with the minimum of diffraction into unwanted orders that otherwise, if allowed, would produce other foci. Calculations show that there is only 0.9% loss of light into unwanted diffraction orders in this condition.

The second example described above with reference to Figures 3 and 4, and each of its variants, has the advantage of a very thin cell structure (calculated to be minimum 3 microns thick with existing liquid crystal materials) so that very small quantities of liquid material are required (around  $100\text{pm}^3$  for a contact lens). This reduces the likelihood of toxic side effects or other forms of bio-incompatibility in the event of leakage or diffusion and largely retaining the mechanical, chemical and gas permeability properties of the isotropic material, which may potentially be a conventional contact lens material.

The liquid crystal used in any of the examples described above may have ferroelectric properties. Ferroelectrics have the advantage of intrinsic bistability,

so that a drive voltage is only required to switch the device; no electrical power is required at other times.

5 In any of the above examples of the device, the electrical control may be achieved by placing the power source and control circuit 4,15 outside the optical area (in the iris area of a contact lens for example). Electrical contact may be made to the liquid crystal by use of electrode patterns similar to those used in a conventional liquid crystal cell.

10 An example of a switching circuit is shown in Figure 5. The output 30 from a photodiode is applied to the respective inputs of two monostables 31, 32 in parallel. The output pulse of one monostable 31 may have a duration of say 120ms and the output pulse of the other  
15 monostable 32 may have a duration of say 80ms. The outputs of the monostables 31, 32 are applied to respective inputs of an Exclusive-Or gate 33. The output of the Exclusive-Or gate 33 is passed to the reset input of a D-type flip-flop 34, the output Q of which provides a switching signal. The  
20 input signal 30 is also passed to the clock input of the flip-flop 34.

If the user blinks for a period of between 80 and 120ms, the output 30 of the photodiode drops for that period. Each of the monostables 31, 32 is triggered. As  
25 the input pulse 30 is low between 80 and 120ms, the Exclusive-Or gate 33 provides a HIGH output during that period to the flip-flop 34, thus toggling the Q output of the flip-flop 34 from HIGH to LOW or vice versa, providing an appropriate switching signal.

30 The bulk of the power requirement is for the drive electronics. With a low leakage integrated device similar in form to that used by an electronic calculator, the power requirement is around 30 microwatts. This is required during the cell switch time. For a ferroelectric liquid  
35 crystal, the switching time is around 10 microseconds. For example, if the user wishes to switch the device once every minute, the average power consumption will be 5pW. This

power must be generated by the photocell or battery. Consider use of a photocell: in a dimly lit room, the optical power available will be around 10% of the bulb rated power, around 10W typically, distributed around a wall area of say  $50\text{m}^2$ , giving an illumination of  $0.2\text{W}/\text{m}^2$ , or 0.2 microwatts/ $\text{mm}^2$ . A 1mm square silicon photodiode has a power conversion efficiency of about 30% in the visible wavelength range and therefore provides 60nW, which is ample average power to switch a ferroelectric device.

A cholesteric device requires a drive voltage of 8 to 10V which preferably on average has little or no DC content (liquid crystals slowly hydrolyse when a DC field is applied to them). If it is assumed that the device has a capacitance of around 150pF, the energy lost each time the potential is reversed, given by  $\frac{1}{2}CV^2$ , is around 7.5nJ. If the device is refreshed every ten seconds, the average power consumption of the cell is 75nW, similar to the power produced by a 1mm square silicon photodiode in dim room lighting.

A battery can also conveniently supply this level of power for long durations. A miniature battery can be constructed using two electrodes of dissimilar materials, preferably metals, whereby the system generates a current when both electrodes are in contact with a common electrolyte. The electrodes may take many forms. They may be printed onto a surface, fabricated from electrode material, or constructed by dispersing particles of the electrode material in an inert matrix such that conduction of electricity may occur across the matrix.

The battery may be produced in an inert state where no current is passed until the battery is immersed in liquid. Such fluid may be the tear film in contact with the eye. This feature may be provided by constructing a battery cell where the whole cell is enclosed, but where a membrane provides access to ions or water from the outside of the device. Water or ions diffusing into the device activates the battery. It may be desirable to utilise a membrane

which does not allow ions from the electrodes to pass across the membrane to the outside of the device.

In one form, the battery consists of two planar electrodes separated by a small gap. In this gap there is held a partially dehydrated gel containing electrolyte. The whole cell is separated from the exterior by a water-permeable membrane. As a result of the partial dehydration, the gel does not fill the gap between the electrodes and no current can pass. When the contact lens comes in contact with the eye, water crosses the selective membrane causing the gel to swell to fill the void. The electrodes are then connected by electrolyte and current flows.

In a second form, the battery consists of two electrodes with a crystalline salt electrolyte held between them. Passage of water across a membrane activates the battery by hydration of the crystalline electrolyte.

In a third form, shown in Figure 6 as an example, the battery consists of a copper electrodes 40 and a zinc electrode 41 separated by a dehydrated polymer electrolyte 42. A selective membrane 43 surrounds the electrodes 40, 41 and wires 44, 45 pass through the membrane 43 to the respective electrodes 40, 41. Hydration of the polymer electrolyte 42 by water passing through the membrane 43 activates the battery. The use of a polymer electrolyte 42 has the advantage that this material has high molecular weight and is therefore readily contained by a membrane. It is possible and desirable to select a membrane material that will allow the passage of water molecules, but that will reject the high molecular weight electrolyte and ions from the electrodes.

In a fourth form, the battery may consist of two electrodes alone. Immersing the system in tear fluid provides the electrolyte required to complete the circuit.

In a fifth form, the battery may consist of two electrodes in contact with a dehydrated gel. Immersion in tear fluid both hydrates the gel and provides the ions for

the electrolyte. The gel helps to localise ions from the electrodes.

5 An organic chelating agent may be provided within those battery configurations having a membrane. This chelating agent may be employed to allow movement of ions within the cell while preventing them from migrating across the membrane.

10 Contact lenses according to the present invention can provide the advantage of allowing the user to select near or distance vision in a simple manner and can reduce or avoid the difficulties associated with simultaneous-vision bifocal lenses while retaining the advantages of bifocal lenses. Mechanical, chemical and gas permeability, and biocompatibility properties are determined by the  
15 encapsulating material which may be a conventional ophthalmic lens material.

CLAIMS

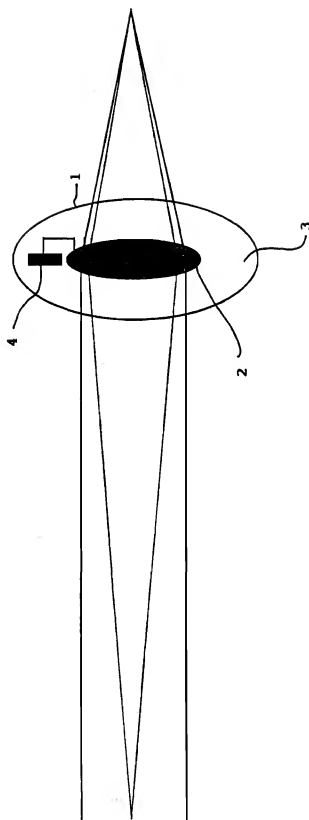
1. A lens assembly (1) comprising:  
a lens (2) having a property which may be switched by  
5 application of an electric or magnetic field, said property  
being at least one of the focal length, absorption, colour,  
and effective aperture;  
switching means (4) to provide a drive impulse to  
switch the property of the lens (2); and,  
10 an integral power source (4) to provide power for the  
switching means.
2. An assembly according to claim 1, wherein the lens  
assembly (1) is sealed, having no external connections.
- 15 3. An assembly according to claim 1 or claim 2, wherein  
the power source is a battery.
4. An assembly according to claim 3, wherein the battery  
20 is operable using tear fluid.
5. An assembly according to claim 1 or claim 2, wherein  
the power source is a photocell.
- 25 6. An assembly according to any of claims 1 to 5, wherein  
the lens includes a birefringent lens (10) and a layer of  
liquid crystal (11).
7. An assembly according to any of claims 1 to 5, wherein  
30 the lens includes a diffractive lens (21) and a layer of  
liquid crystal (22).
8. An assembly according to claim 6 or claim 7, further  
comprising a polariser (13).
- 35 9. An assembly according to any of claims 6 to 8, wherein  
the liquid crystal is nematic.



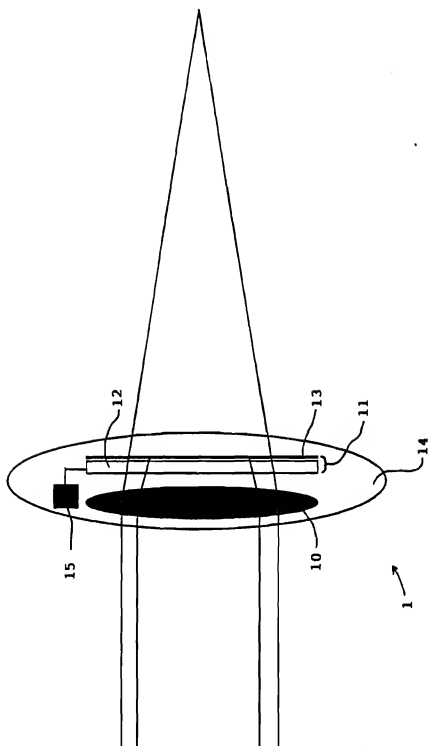
10. An assembly according to any of claims 6 to 8, wherein the liquid crystal is cholesteric.
11. An assembly according to any of claims 6 to 8, wherein  
5 the liquid crystal is ferroelectric.
12. An assembly according to any of claims 6 to 8, wherein the liquid crystal contains a dichroic dye.
- 10 13. An assembly according to any of claims 1 to 12, wherein the assembly is an ophthalmic lens.
14. An assembly according to any of claims 1 to 13, wherein the switching means includes means (30,31,32,33,34)  
15 for detecting a drop in the level of ambient light and changing the focal length of the lens when the detected light level drops for longer than a predetermined period of time.
- 20 15. An assembly according to any of claims 1 to 5, wherein the assembly is a contact lens or an intra-ocular lens.
16. An assembly according to claim 15, wherein the lens includes a diffractive lens (21) and a layer of liquid  
25 crystal (22).
17. An assembly according to claim 15 or claim 16, wherein the lens is switchable between two different focal lengths, independent of polarisation, by the application of an  
30 electric field.
18. An assembly according to claim 17, wherein the lens transmits at least 90% of incident light at each of the two focal lengths.
- 35

19. An assembly according to claim 17, wherein the lens transmits nearly 100% of incident light at each of the two focal lengths.
- 5 20. An assembly according to any of claims 15 to 18, wherein the switching means is activated by a deliberate blinking of the eye of a user for an extended, predetermined period of time.
- 10 21. An assembly according to claim 20, wherein the switching means includes means (30,31,32,33,34) for detecting a drop in the level of ambient light and changing the focal length of the lens when the detected light level drops for longer than said predetermined period of time.
- 15 22. An assembly according to any of claims 16 to 21, wherein the lens assembly is a contact lens.

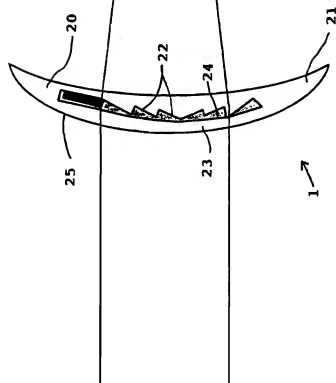
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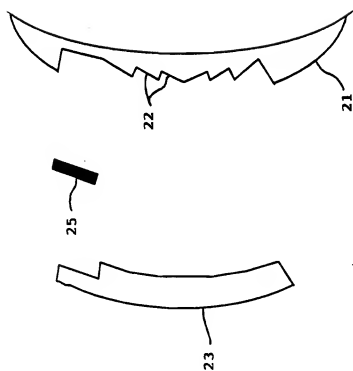
**Figure 1**

2/6

**Figure 2**

3/6

**Figure 3**

**Figure 4**

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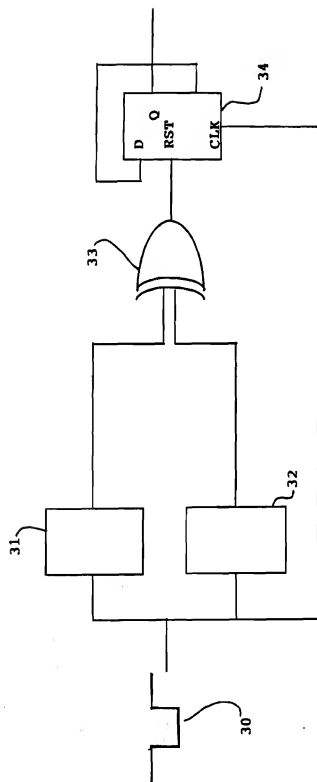
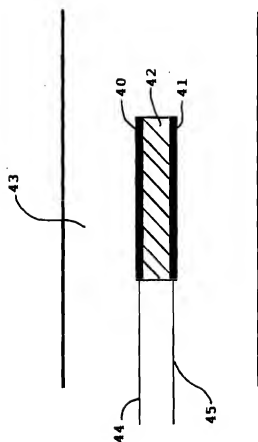


Figure 5

6/6

**Figure 6**



A. CLASSIFICATION OF SUBJECT MATTER  
IPC 5 G02F1/29 G02C7/10

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B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 5 G02F G02C

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	PROCEEDINGS OF THE SPIE, vol.601, December 1985, CANNES, FR pages 155 - 158 S.P. KERN: 'Bifocal, electrically switched intraocular and eyeglass molecular lenses'	1,2,6-9, 13-16, 20-22
A	see the whole article ---	17
X	US,A,4 968 127 (J.P. RUSSELL ET AL.) 6 November 1990	1,3,5,6, 8,13 7,9-12
A	see column 1, line 51 - column 3, line 37 see figures 1,2 --- -/-	

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☒ Patent family members are listed in annex.

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C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X A	GB,A,2 170 613 (OLYMPUS OPTICAL CO LTD (JAPAN)) 6 August 1986  see page 1, line 65 - page 2, line 90 see figures 1,3 ---	1,3,6,8, 13 7,9-12
X A	US,A,5 184 156 (M. BLACK, V. KUPERSHMIDT) 2 February 1993  see column 2, line 32 - line 54 see column 3, line 43 - column 5, line 11 see figures 1,2 ---	1,3,6,8, 9,11,13 7,10
X A	US,A,5 015 086 (E. OKAUE ET AL.) 14 May 1991  see column 2, line 33 - line 68 see column 5, line 56 - column 7, line 31 see figure 2 -----	1,5,6,8, 9,13 7,10-12

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